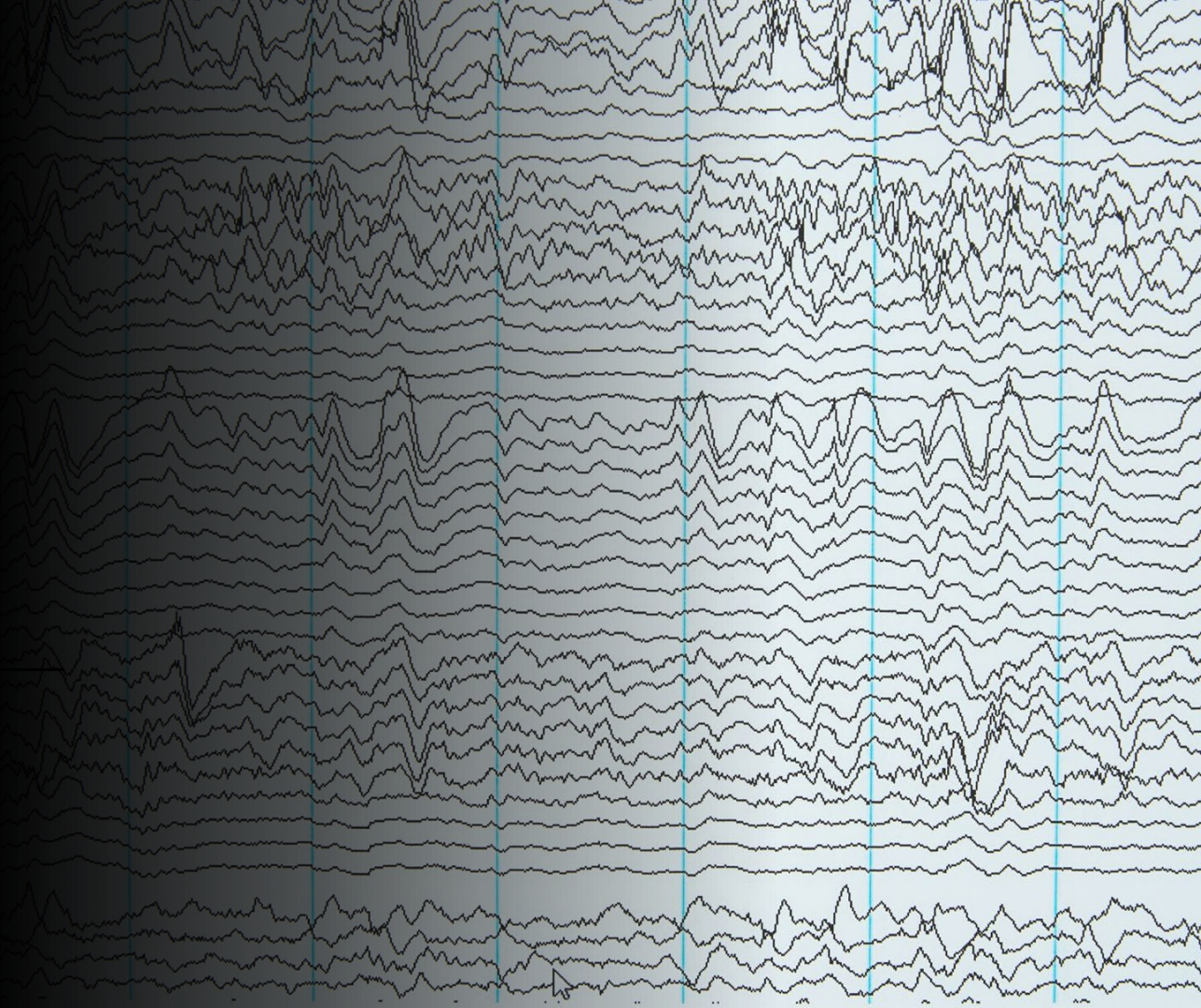


# Mice Sleep Staging from EEG and EMG signals

ECE 408 Project Presentation  
Fazla, Paul, Yixuan, Yanlong





# Introduction: Background and Motivation

## Sleep Staging and Its Importance

- Sleep, a fundamental behavior with vast biological implications, is typically classified into stages: Wakefulness, REM, and non-REM.
- Understanding sleep stages is critical for both preclinical and clinical research, providing insights into sleep architecture and related disorders for mice.

# Introduction: Background and Motivation

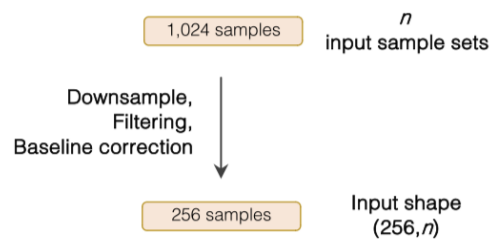
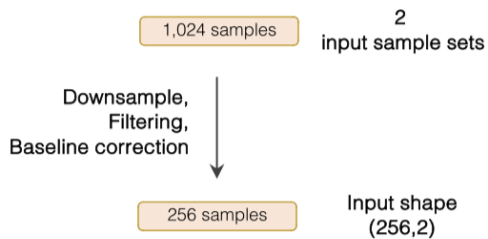
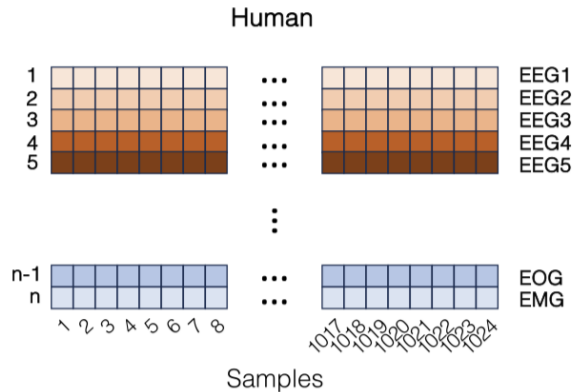
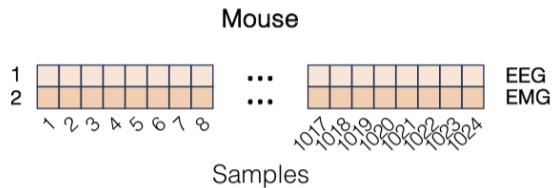
## Challenges in Sleep Staging

- Traditional methods are labor-intensive and require expertise, making automated solutions a necessity.
- However, current automated methods face challenges, such as larger resolution (4 sec - 10 sec) and a lack of unified models that can handle various input sources.

## Literture review

The research paper by Justus T. C. Schwabedal et al. focuses on sleep stage classification and EEG **artifact detection** in mice using a deep neural network model  
artifact-free data VS artifact data

Research by Akara Suprata et al. introduces a deep learning model that utilizes **Convolutional Neural Networks (CNNs)** to extract **time-invariant features** from raw single-channel EEG data



Connection between mice and human

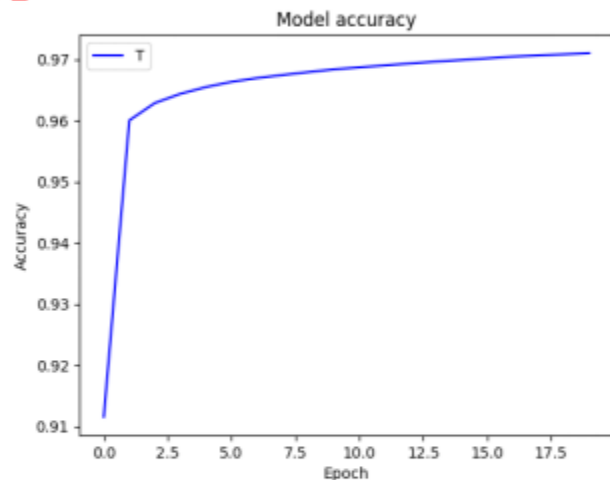
# Baseline and Implement

## A novel approach- **SlumberNet**

Implementation of the SlumberNet

Residual Neural Network

Data preprocess

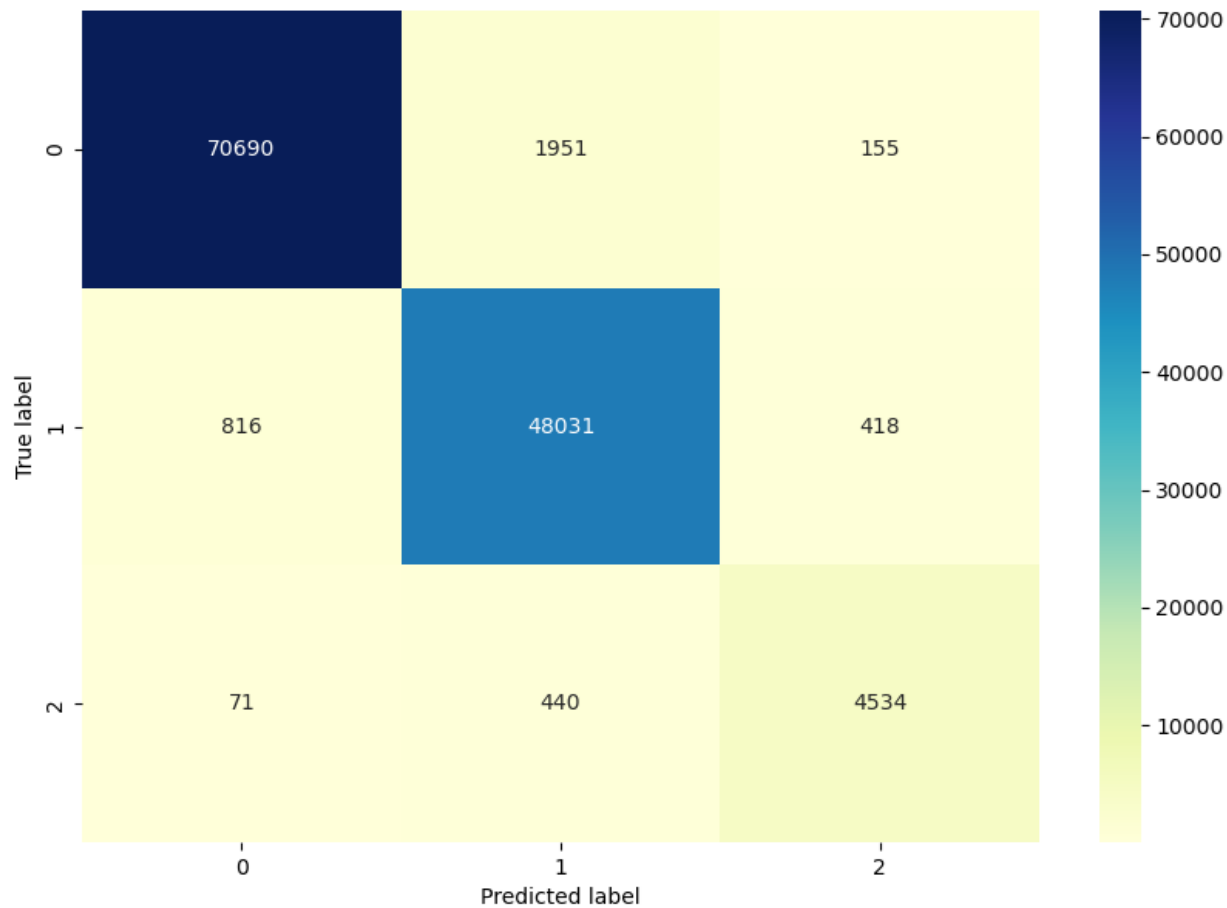


Epoch 20/20

4966/4966 [=====] - 435s 88ms/step - loss: 0.0838 - accuracy: 0.9710 - lr: 1.0000e-06

complex

Confusion Matrix for Fold 1



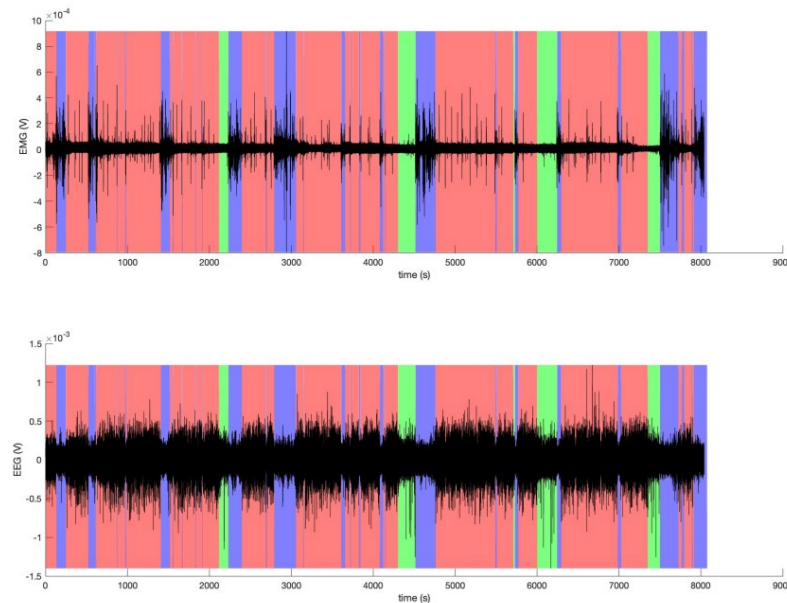
# Dataset

## Data Collection

- The dataset comprises electrophysiological **time-series data, specifically EEG and EMG** signals collected during sleep studies on mice.
- Expert annotations provide second-by-second sleep stage labels corresponding to Wake, SWS (slow-wave sleep), or REM (rapid eye movement) states.

## Memory-enhancing properties of sleep depend on the oscillatory amplitude of norepinephrine

Celia Kjaerby<sup>1,2,5</sup>, Mie Andersen<sup>1,2</sup>, Natalie Hauglund<sup>1</sup>, Verena Untiet<sup>1</sup>, Camilla Dall<sup>1</sup>, Björn Sigurdsson<sup>1</sup>, Fengfei Ding<sup>2,3</sup>, Jiesi Feng<sup>4</sup>, Yulong Li<sup>4,5,6</sup>, Pia Weikop<sup>1</sup>, Hajime Hirase<sup>1</sup> and Maiken Nedergaard<sup>1,2,5</sup>







# Dataset

## **Dataset Statistics**

- Subjects: Data from 8 mouse subjects, both male and female.
- Sampling Rate: EEG and EMG signals sampled at 512 Hz.
- Duration: Approximately 4 hours per subject, leading to millions of data points.
- Labels: Expert-scored stages for rigorous evaluation.

## **Data Preprocessing**

- Irregularity Removal: Periods with uncertain stage classification are excluded to ensure data consistency.
- Notch filtering
- Bandpass filtering EEG (.5 to 70 Hz), EMG (1 to 250 Hz)
- Subject-wise Normalization: Signal normalization accounts for individual variability in electrophysiological signal features.
- Temporal Slicing: Signals are segmented into one-second epochs to match the temporal resolution of sleep stage labels.

# CNN-based model

## Design Approach

Utilize 1D convolutional layers to extract temporal features from raw time-series data.

Apply ReLU activation for non-linearity and Batch Normalization to stabilize training.

Implement Dropout for regularization and to prevent overfitting.

## Architecture Components:

### Raw Signal Pathways (EEG & EMG):

1. Capture features from raw EEG and EMG signals.
2. Sequential layers of 1D convolutions with progressive downsampling.
3. Adaptive Average Pooling to convert feature maps into a flat vector.

### Fourier Transformed Signal Pathways (FFT-EEG & FFT-EMG)

1. Process FFT-transformed signals to exploit frequency domain information.
2. Similar layer structure as raw signal pathways for feature extraction.

## Output Layer

1. Concatenates outputs from all pathways.
2. Final classification performed with fully connected layers.

```
def conv_1d(ni, nf, kernel_size, stride, padding, drop=None):
    return nn.Sequential(
        nn.Conv1d(ni, nf, kernel_size=kernel_size, stride=stride, padding=padding),
        nn.PReLU(),
        nn.BatchNorm1d(nf),
        nn.Dropout(drop) if drop else nn.Identity()
    )

# Modify the Classifier class for regular 1D convolutions
class Classifier(nn.Module):
    def __init__(self, raw_ni_EEG, fft_ni_EEG, raw_ni_EMG, fft_ni_EMG, no, drop=.5):
        super().__init__()

        self.raw_EEG = nn.Sequential(
            conv_1d(raw_ni_EEG, 32, 8, 1, 3, drop=drop),
            conv_1d(32, 64, 3, 1, 1, drop=drop),
            conv_1d(64, 128, 8, 2, 2, drop=drop),
            conv_1d(128, 128, 3, 1, 1, drop=drop),
            conv_1d(128, 256, 8, 2, 2),
            conv_1d(256, 256, 3, 1, 1),
            nn.AdaptiveAvgPool1d(1),
            nn.Flatten(),
            nn.Dropout(drop),
            nn.Linear(256, 64),
            nn.PReLU(),
            nn.BatchNorm1d(64)
        )
    )
```

# Result for CNN-based Approach

Class Name	Precision	1-Precision	Recall	1-Recall	f1-score
Awake	0.8414	0.1586	0.9321	0.0679	0.8844
NREM	0.9177	0.0823	0.8518	0.1482	0.8835
REM	0.4629	0.5371	0.5413	0.4587	0.4990

Awake:NREM:RE  
M(4:8:1)

Mice	CNN-Based model
1	90.92
2	82.3
3	87.97
4	83.23
5	89.83
6	91.2
7	71.73
8	84.79
Avg	85.5

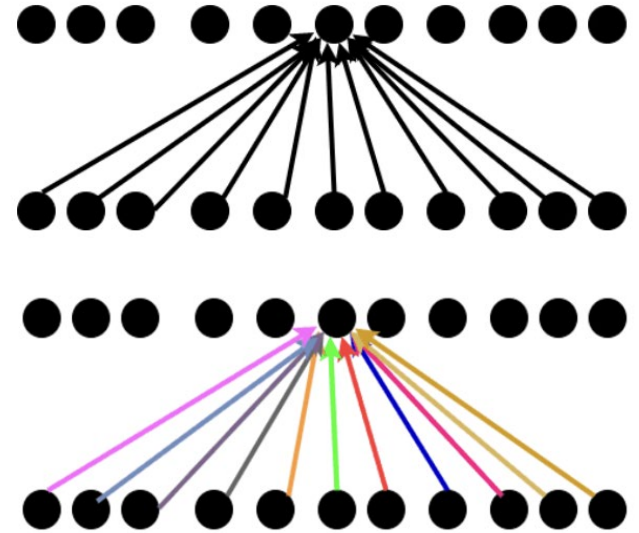
Training Set				
TARGET \ OUTPUT	Awake	NREM	REM	SUM
Awake	32895 29.57%	6073 5.46%	127 0.11%	39095 84.14% 15.86%
NREM	2258 2.03%	58863 52.91%	3019 2.71%	64140 91.77% 8.23%
REM	138 0.12%	4169 3.75%	3712 3.34%	8019 46.29% 53.71%
SUM	35291 93.21% 6.79%	69105 85.18% 14.82%	6858 54.13% 45.87%	95470 / 111254 85.81% 14.19%

# Adding Attention mechanisms

- Using self-attention for contextual learning
  - The past/future stages affect probabilities of current stage

## Architecture:

- Placed after 1D convolutional layers for more global context
- Tuned number of embeddings and heads for different datasets



# Adding Attention mechanisms

## Results:

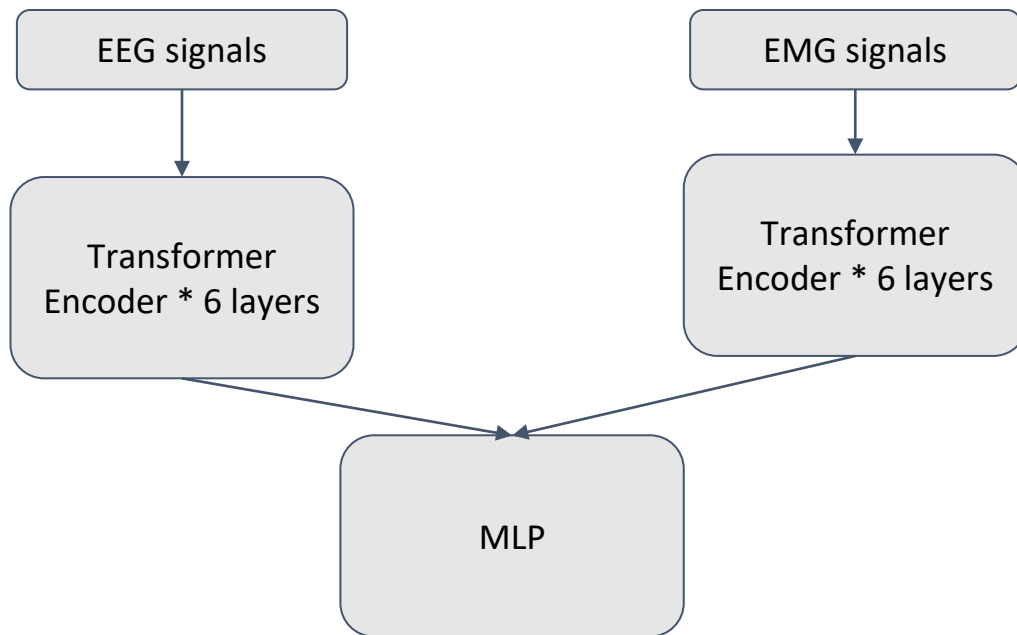
- Slight decrease in average accuracy:
  - 85.5% -> 84.65%
  - Limitation in dataset size
  - REM precision decreased

Class Name	Precision	1-Precision	Recall	1-Recall	f1-score
Awake	0.7725	0.2275	0.8558	0.1442	0.8120
NREM	0.9064	0.0936	0.8087	0.1913	0.8548
REM	0.2667	0.7333	0.4084	0.5916	0.3227

## Confusion matrix:

Training Set				
TARGET \ OUTPUT	Awake	NREM	REM	SUM
Awake	30202 27.14%	7219 6.49%	1674 1.50%	39095 77.25% 22.75%
NREM	3389 3.05%	55895 50.24%	2383 2.14%	61667 90.64% 9.36%
REM	1700 1.53%	6001 5.39%	2801 2.52%	10502 26.67% 73.33%
SUM	35291 85.58% 14.42%	69115 80.87% 19.13%	6858 40.84% 59.16%	88898 / 111264 79.90% 20.10%

# Transformer-based model - Model architecture



# Transformer-based model - Results

Index	1	2	3	4	5	6	7	8	Average
ACC (%)	77.88	85.20	62.25	51.42	80.37	84.29	82.27	84.76	76.05

Matrix	Avg-acc	Avg-precision	Avg-recall	avg-specificity	Avg-F1
Result	76.05%	0.5382	0.5307	0.8285	0.4997

# Transformer-based model - discussion

Result discussion:

Transformer-based models tend to underperform compared to traditional CNN-based models when data is limited, as transformers require larger datasets to achieve optimal results.



# Limitations

- Amount of data
  - Only 8 mice
  - Impacts attention and transformer performance
- Quality of data
  - Class imbalance
  - Impacts REM performance

# Future work

- Investigating different species of mice
  - General model
- Detecting changes in sleep stage
- Combine transformer and CNN models
- Generating synthetic data to overcome class imbalance
  - REM sleep data is limited

Questions?